



# MAGNETO-ELECTRIC NANOPARTICLES – A NEW DRUG DELIVERY SYSTEM

**Deven. S. Aspalani\*, Ashutosh. S. Deshmukh, Sakshi.P.Deore, Gayatri. A. Pandit,  
Meghraj.S. Deshmukh.**

**Dr. Kolpe Institute of Pharmacy, Kolpewadi, Kopergaon, Maharaashtra, India.**

Corresponding Author Mail- [99devenaspalani@gmail.com](mailto:99devenaspalani@gmail.com)

## Abstract

Magneto nanoparticles( MNPs) have evolved extensively during recent times, in part due to the rapid-fire expansion of nanotechnology and to their active magnetic core with a high surfaceto- volume rate, while their face functionalization opened the door to a plethora of medicine, gene and bioactive patch immobilization. reining the high reactivity of the glamorous core was achieved by Colorful functionalization ways, producing MNPs acclimatized for the opinion and treatment of cardiovascular or neurological complaint, excrescences and cancer. Superparamagnetic iron oxide nanoparticles SPIONs) are established at the core of medicine-delivery systems and could act as effective agents for MFH( glamorous fluid hyperthermia). Depending on the functionalization patch and natural morphological features, MNPs now cover a broad compass which the current review aims to overview.

**Keywords** Magnetic nanoparticle, MRI, nanomedicine, Drug delivery system

## Introduction

Magnetic nanoparticles( MNPs) are at the veritably core of magnetic delivery systems and they aim to attack point-specific excrescences while immaculately swinging a controlled- release profile suitable for complaint treatment. Their multifunctional dimensionality makes it possible for MNPs to be used in nanomedicine as optional campaigners for medicine targeting remedy when using an externally applied magnetic field [1,2].

With tuneable physio- chemical parcels and a veritably high face- to- volume rate typical for nanoparticles, MNPs can be finagled into medicine- delivery systems with analogous sizes to the organism's own antibodies or proteins for bettered biocompatibility, while incorporating remedial agents that would else be delicate to deliver to the cancer cells. When superparamagnetic nanoparticles( SPIONs) are carpeted with biologically compatible polymers of adipose acids, systems with bettered colloidal stability and reduced tendency of aggregation are attained [3]. MNPs were also used as discrepancy agents in magnetic resonance imaging( MRI). When functionalized with epithelial growth factor the receptor antibodies or aptamers, an effective opinion tool is created for numerous types of cancer or Indeed discovery of brain inflammation. MNPs are being used as indispensable discrepancy agents in MR imaging owing to their superparamagnetic parcels and high reflexivity, doubled by high biocompatibility upon face functionalization and low toxin into the bloodstream[4,5,6].

The pledge of feasible campaigners in cancer treatment made exploration in the field of MNPs flourish and moment hundreds of reports are published annually describing new or bettered strategies for using MNP systems in complaint treatment. Conjugation of IONs magnetite and maghemite are generally stylish

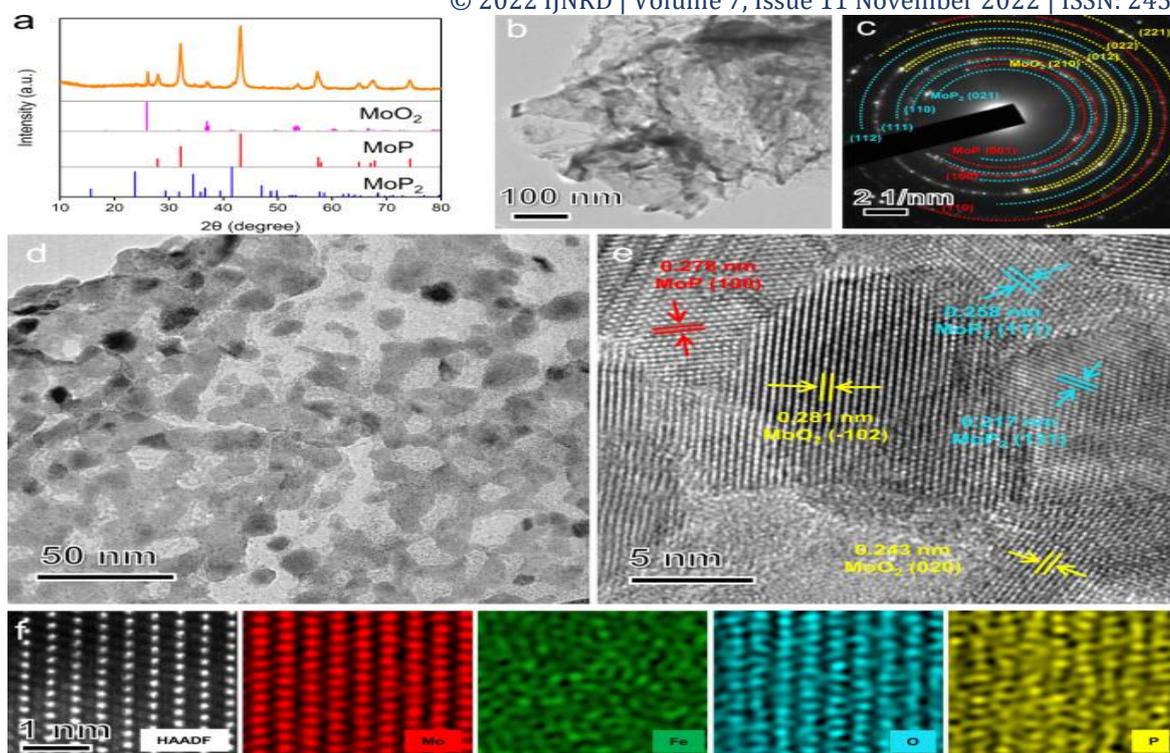
permitted) with medicines yields medicine- loaded IONs that can be directed using an external glamorous field to the point where the excrescence cells live, and this medicine- delivery variant is nominated glamorous medicine targeting( MDT). The variety of similar approaches would make a comprehensive review relatively delicate and lengthy, hence the current review focuses on the most advances with MNPs over the once three times [7,8,9].

## 1.MR Imaging

MRI is an on-invasive imaging fashion that exploits the capability of protons to align and process around  $B_0$  (an applied glamorous field) and to relax when perturbed from  $B_0$  by the operation of a transverse radiofrequency. This relaxation process comprises two distinct terms T1- recovery or longitudinal relaxation( positive discrepancy improvement, sensitive to MNPs consistence, hence effective only for thin coatings) and T2- decay or transverse relaxation( favoured by MNPs high vulnerability, negative discrepancy- enhanced, utmost used for SPIONs) [10,11]. This exploration direction is also motivated by the need to replace current discrepancy agents grounded on Gd3 complexes, which pose worrying health issues and uninvited side Goods. As precious MRI discrepancy agents, SPION nanoparticles have gained increased attention and fission ability, especially iron oxide- grounded. Relaxivity is a direct and quantifiable measure of a discrepancy agent's effectiveness  $R_1(1/T_1)$  and  $R_2(1/T_2)$ , and depends on the type of MNPs used, applied field and temperature [12,13,14].

Besenhart et al. have demonstrated a reproducible SPION conflation in an inflow reactor using aco-precipitation system using dextran as the face content agent, followed by quenching( by timely 2 – 100 s addition of 0.32 M citric acid result- stops nucleation due to chelation of iron ions) after the conformation of the asked iron oxide core, achieving nanoparticles of lower than 5 nm. The longitudinal reflexivity ( $r_1 = 10.7 - 12.4 \text{ mM}^{-1} \text{ s}^{-1}$ ) and transversal reflexivity achieved  $r_2 = 20.5 - 57.2 \text{ mM}^{-1} \text{ s}^{-1}$ ) recommend this synthetic procedure to produce affordable SPIONs as effective MRI T1 discrepancy agents and reserves for Gd- grounded bones ( of lower  $r_1$  in marketable Dotarem<sup>TM</sup> or Gadovist<sup>TM</sup>,  $4.2 - 5.3 \text{ mM}^{-1} \text{ s}^{-1}$ ) [9].

Some general introductory reviews covering MRI imaging have surfaced in the literature. Running the response at 60 C, the swab co-precipitation to form spinel phases (magnetite/ maghemite) verified by real-time XRD data that intermediate ferrihydrite species transfigure fleetly into the final spinel. crucial aspects that impact the effectiveness of iron oxide NPs in MRI include magnetization, size, effective compass, inhomogeneity of girding generated glamorous field, demitasse phase, collaboration number of water, electronic relaxation time, and face revision. T2 reflexivity for case can be increased by synthesizing SPIONs with bettered MS and effective compass. still, lately another iron- grounded emulsion was delved as a new agent for enhanced hyperthermia remedy and a T2 discrepancy agent for MRI operation iron nitride 0- Fe4N nanoparticles, which parade three times advanced achromatism magnetization and could also be Duly covered by an oleic acid subcaste for farther functionalization [15,16,17].



Chelating ligands similar as DoS( deblock polymer PDOPA- b- PSar) were shown to bind to Mn<sup>2+</sup> centres to form new, invariant micelles Mn<sup>2+</sup>@PDOPA- b- PSar of 73.4 nm size low polydispersity indicator PDI = 0.159) that were delved as MRI discrepancy agents with good discrepancy features in imaging owing to the glamorous manganese core[17,18,19]. These micelles showed good results in MRI tests as T1- ladened discrepancy agents with reflexivity  $r1 = 27.7 \text{ mM}^{-1}\text{s}^{-1}$ , and showed promising results for other biomedical operations similar as medicine release systems, while in vivo tests performed on rats showed cell survival rates advanced than 70[20,21].

The occasion of using MNPs as discrepancy advancements in MR imaging proves a current content of interest, as the results are veritably detailed and the irradiation impact is reduced to a minimum. Specific goods of coatings( with amine- carrying motes) on MNPs ' performance in MRI revealed intriguing improvement goods, and exemplifications include coating with sodium oleate, chitosan or organic acids, as well as amino halves poly( acrylamide) coatings[23,24].

## 2. Magnetic Nanoparticles for brain delivery

Nanomedicines for rectifiers have opened instigative prospects for medicine delivery systems due to their capability of target( cells/ organs) specific delivery and release. Among NCs, glamorous NPs( M- NPs) are considerably employed medicine delivery NCs due to their unique parcels similar as glamorous hyperthermia, and controllable movements and MRI discrepancy agent [25,26]. The favourable medicine delivery parcels of M- NPs are their covert face chemistry, high medicine- lading capacity, multiple functionalities and optimal flyspeck sizes( 10 – 100 nm). Sagar etal. have explained the possible medicine release medium of medicine-loaded M- NCs upon external stimulation similar as thermal responsive, optic responsive, pH responsive, enzymatic catalysis and aural activation [27,28]. M- NCs- grounded molecular transport has been espoused as ultramodern approach to increase delivery with reduced toxin in numerous fields that is, cardiology, ophthalmology and oncology. As recent advancements, sweats are being made to deliver medicine at neuronal position across the BBB. The delivery of remedial agents across the brain is veritably limited and until now technologies to acclimate their pharmaco- distribution have remained defined. Hence, there's a need to develop the new strategies for point-specific delivery of remedial agents across the complete BBB with minimum toxin remains a challenge in the field [29,30,31].

Advances in material wisdom for controlling glamorous parcels, size and shape of M- NCs via espousing new conflation routes expand the protocol toward developing effective remedial agent to cure conditions. The preface of external glamorous force- grounded detector for medicine delivery and controlled release in the brain is the recent disquisition. In this approach, the speed and time for medicine delivery is estimated on

applying external glamorous field. Several experts reported the capabilities of M- NCs for the advance medicine delivery and proposed M- NCs as excellent substantiated nanomedicine carriers. Pilakka-Kanthikeel et al. showed an in vitro study using M- NCs for targeted brain- deduced neurotropic factors( BDNF) delivery across the BBB. Delivering BDNF helps in precluding the HIV- related neurotoxicity and complaint progression in case of Neuro AIDS. Authors developed Fe<sub>3</sub>O<sub>4</sub>- NCs for binding with BDNF and assessed efficacy and capability to transmigration across the BBB using an in vitro BBB model. The issues of this study suggested that transmigrated BDNF is effective in suppressing the morphine- convinced apoptosis, converting response element- list expression and restoring the chine viscosity. similar developed NCs may give an implicit remedial approach to treat drowsy dependence , cover neurotoxicity and synaptic viscosity degeneration. Ding et al. developed a new transferrin- bedded fluorescent multifunctional liposomal glamorous NCs expression to enhance BBB transmigration. A binary medium that includes receptor agreement combined with external non-invasive glamorous force incorporated into homogenous magneto-liposome(100 nm) was used to ameliorate delivery across BBB The glamorous - liposome expression demonstrated improves delivery across BBB than traditional styles. Authors also suggested the need of in vivo studies to clarify the affiliated medium of binary transportation for the successful operation of these NCs in colourful CNS conditions [32,33,34].

### 3.Magneto-electric nanocarriers

This challenges allows the control of magnetization and electrical polarization in a single phase. Energy conversion from magneto to electric takes advantage of piezoelectric parcels of the ferroelectric phase and piezomagnetic parcels of the ferromagnetic phase, crucial advantages of ME- NCs over M- NCs are structurally compatible, high stability( chemical, thermal and mechanical) and easy medication. In general, ME- NCs are core shell structures, wherein a glamorous core is saved with a shell of asked electrical parcels. The control on core size and consistence of the shell enables the fine adaptation of the structure and phase bit of the ME- NCs expression, preceding in accoutrements with tuneable parcels and reproducible features [35,36,37]. The conflation of core – shell NPs is conventionally carried out in two consecutive way I) the rush of the ferrite NPs; and ii) the creation of a shell around each NP. Along with medicine delivery, ME nanostructures due to over- mentioned unique parcels have been used in transduction, spintronics, optic bias and detectors. also, ME- NCs are dispersion-free, energy-effective and low- field on- demand targeted medicine release can be achieved by applying low remote ME field. still, ME nanostructures can be of inorganic – inorganic nano- compound and organic- essence oxide fabrics. ME- NCs enable a new dissipate ion-free medium to force a high- efficacy externally controlled medicine release process at the subcellular position using remote low- energy direct current and/ or interspersing current(a.c.) [38,39,40].

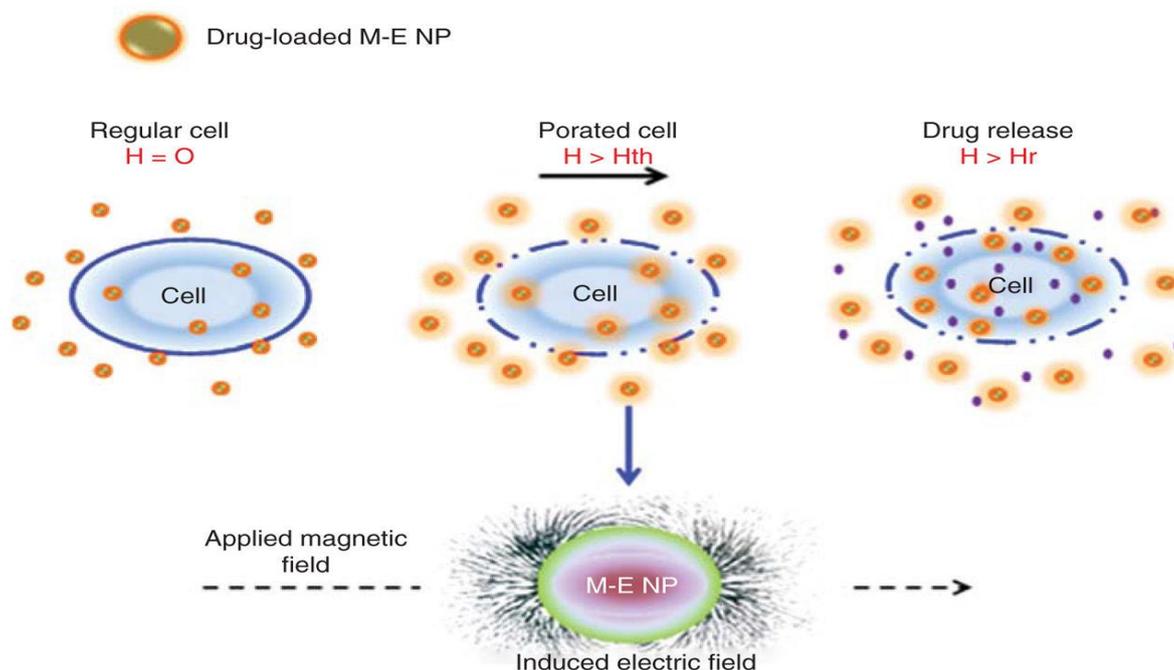
For the first time, Dr. Nair's group in collaboration with Dr. Khizroev explored the use of computational technology in prognosticating the artificial stimulation of neurons using the ME- NCs in deep inside the brain. Yue et al. demonstrated this conception and proposed this non-invasive fashion that couples' neuronal electric signals to the glamorous dipoles of ME- NCs. The established protocol is of use for non-invasive stimulating the patient brain with Parkinson's complaint to bring the palpitated sequences of the electric field to the situations similar to those of healthy people. Simulation results prognosticated that ME- NCs attention of  $36 \times 10^6$  patches/ cc with size of 20 nm and frequency( 80 Hz) of the externally applied glamorous field( 300 Oe) can give us the asked goods. Field- controlled ME- NP medicine expression showed a unique capability of field- touched off release across BBB due to natural magnetoelectricity. On applying external glamorous field, the electric forces in medicine- NCs bonds enable ever controlled delivery due to coupling of ME parcels. The operation of ME- NCs for filed- controlled point-specific and on- demand medicine delivery with possible delivery and release medium is banded in coming section [41,42].

### 4.Potentials of ME-NCs in drug delivery

ME- NPs are exploring for field- controlled medicine delivery and on- demand release operation. ME- NCs can be synthesized in different size and shape depending upon the use and target organ that is, globular core – shell NPs( glamorous core and an electric shell) or rods with a piezoelectric coating( concentric glamorous / piezoelectric tubes) or compound sphere( piezoelectric pottery or piezopolymers with girdled M- NPs). Only

many reports are available on ME- NCs- grounded medicine delivery and other natural-affiliated operations[44].

Another implicit operation of ME- NCs was explored by Nair et al. for anti-HIV medicine delivery. Authors used ME- NCs for successful on- demand delivery of ARV medicine across the BBB for the forestalment of Neuro AIDS( 65). The proposed medium of medicine lading and on- demand release under the effect of external glamorous field is illustrated in Figure 4. Results of using in vitro model demonstrate on- demand release of azidothymidine 50- triphosphate( an anti-HIV medicine) using  $\text{CoFe}_2\text{O}_4@ \text{BaTiO}_3$ (30 nm) NPs was achieved via operation of low a.c. glamorous field across the BBB. Authors proposed that this platform technology of on- demand medicine delivery can be used for other CNS conditions treatment, where deep towel high efficacy at subcellular position is demanded [44].



The controlled electric field of ME- NCs via external glamorous field can be explored to exploit the natural parcels of the cell membrane. Ion channels present on cell membrane are kind of electrically concentrated medium that can be affected by the applied electric field. This property explored to open up the pores of cell membrane on applying electric field. The porosity of the cell membrane is set up to be dependent of applied electric field. Guduru et al. used this field- controlled nano- electroporation( the scale down of electroporation to nanoscale is appertained as nano- electroporation) fashion for medicine delivery using glamorous filed actuated ME- NCs loaded with anticancer medicine inside the excrescence cell. medicine- loaded ME- NCs are able of to induce enough localized field demanded to open up the cell membrane pores for the penetration of NCs and medicine release on changing field without causing heat. Authors explored nano- electroporation via using  $\text{CoFe}_2\text{O}_4@ \text{BaTiO}_3$ ( 30 nm) ME- NCs for controlled and targeted medicine delivery to annihilate ovarian cancer. A physical conception is explored grounded on the differences in the electrical parcels of excrescence cell membrane, healthy cells membrane and the capability of ME- NCs transformers of remote glamorous field energy into the ME- NCs natural electric field energy. An in vitro model on mortal ovarian melanoma cell( SKOV- 3) and healthy cell( HOMECE) lines was used for the evidence- of- conception using electroporation fashion( cell membrane-dependent electrical system to spark medicine delivery into the cells). Results showed that an electric field  $> 1000 \text{ V/cm}$  creates pores of applicable size for the penetration of nano formulation through the cell membrane. medicine- loaded ME- NCs( $\text{CoFe}_2\text{O}_4@ \text{BaTiO}_3$ ) entered through the membrane on applying 30 Oe to spark largely specific uptake of paclitaxel and fully cancelled the excrescence within 24 h without any side effect. A field- controlled gate generated on commerce between ME- NCs and the electric system of the membrane allows the medicine- loaded ME- NCs into the excrescence cells as depicted in Proposed scheme highlights the nano- electroporation methodology using ME- NCs and medicine release pattern. The eventuality of cancer cell is lower than that of healthy cell, likewise the threshold field(  $H_{th}$ ) for medicine- loaded ME- NCs is lower in case of cancer cell than healthy one. Using simple isotropic expression that is,  $DP$ ( convinced electric dipole field) =  $\alpha H$ ( external glamorous field), the ME measure(  $\alpha$ )

is calculated as  $100 \text{ mV cm}^{-1} \text{ Oe}^{-1}$ , which can be attained at small glamorous field( 100 Oe). On applying applicable glamorous field( 100 Oe), the medicine- loaded ME- NCs access the cell membrane via electroporation and farther medicine can be released from ME- NCs on adding field to critical value that is, Hr. To achieve the high- efficacy uptake, Hr should be advanced than Hth. For the particularity of uptake to the cancer cell, the value of applied external field HA should be advanced than Hr- cancer and lower than that of Hth-healthy [43].

## 5. Biocompatibility and Toxicity

Biocompatibility and toxin features of anti-cancer phrasings are currently treated with equal care and completely delved hourly; endocytosis is not an easy task because colourful vulnerable responses from the cells can putrefy the nanocarrier before entering the cell membrane. Biomimetics was deteriorate as a tool to simplify the objectification of MNPs into living tissue [45,46].

Liposomes act the structure of cell membranes and are globular vesicles composed of multiple phospholipid bilayers, and the objectification of MNPs or SPIONs into similar vesicles can ease the design and effectiveness of medicine- delivery systems since both hydrophilic and lipophilic medicines can be reprised. Liposome use was expanded to vaccine expression and stabilization. This bio-inspired strategy generally affords nippy entry of the medicine by endocytosis with no to minimum damage [47,48].

Cytotoxicity- Hourly, the remedial effect was the main concern of the clinician; still, the toxin that MNPs can have towards bordering towel or during its magnetically- guided path to the excrescence point is less delved , yet is just as important. The non-magnetic shell generally covering MNPs was shown to be essential to the reduced overall toxin of polymer- carpeted essence oxide- grounded MNPs, medicine- loaded nanoparticles or that of bare MNPs and deduced ferrofluids with natural administration applicability [49,50]. The antioxidant effect was assessed by recent reviews in relation to the implicit toxin issues of MNPs. The effect of  $\text{CoFe}_2\text{O}_4$  on Channel catfish ovary cells was reported in 2022 by Srikanth etal. still, magnetite  $\text{Fe}_3\text{O}_4$  can reduce  $\text{CdCl}_2$ - convinced toxin by oxidative stress as shown in a test on small intestine cells of mice, while orally administered nano-  $\text{Fe}_3\text{O}_4$  showed no toxin at all [51,52]. The biodistribution and cytotoxicity of oral iron supplements, which are particularly applicable for cases suffering from iron- insufficiency- convinced anemia, have been delved, and the effect on the mortal adipose towel- deduced stromal cell system of veritably small SPIONs or targeting Parkinson's complaint [53]. Other coatings of magnetite showed no gene toxin, making them suitable campaigners for biomedical operations when guar goo- carpeted  $\text{Fe}_3\text{O}_4$  MNPs attained by co-precipitation(  $\text{Fe}_3\text{O}_4$ - GG nanocomposites) were used on *Drosophila melanogaster*( fruit cover), a leading brute model system used in growing exploration. Regarding anemia treatment options, MNPs are now available in a commercially, FDA- approved medicine expression, ferumoxytol (Feraheme as brand name), with intravenous administration [54,55,56].

## 6. Future Challenges

The development of effective styles to enhance bone mending, rejuvenescence, and conformation of strong cling with artificial implants has always been among the most important exploration areas. Although intriguing bone form strategies have formerly been developed, elaboration of new smart accoutrements as artificial implants is still grueling because successful implantable accoutrements for bone towel engineering must meet a specific set of conditions similar as bioactivity, biocompatibility, mechanical strength and abidance, microstructure and porosity, as well as other important functional parcels similar as a quick response with its terrain once being implanted [57,58,59].

There live colourful ME mixes for towel engineering operations, which have been developed and studied so far. As an illustration, Cold-blooded pulpits of PHBV and cobalt ferrite nanoparticles after the declination of the polymer due to the exposition of the  $\text{CoFe}_2\text{O}_4$  revealed felicity for magneto- and electroactive towel engineering operations. still, cytotoxic goods may do when the glamorous cobalt ferrite nanoparticles demanded for magnetoactive operations are released. Therefore, the negotiation of cobalt ferrite by biocompatible ferrites, similar as  $\text{Fe}_3\text{O}_4$  or poisonous element-free ferrites, e.g.,  $\text{MnFe}_2\text{O}_4$ , should be delved . In this case, non-toxic paddings being released will give no implicit cytotoxic effect on cells. In addition,  $\text{Fe}_3\text{O}_4$  nanoparticles are the only essence oxide nanoparticles approved by FDA for clinical use, therefore, a

wide operation of ME nanoparticles should face the challenge of FDA blessing. also, mechanical Parcels of the ME mixes can deteriorate, similar as compressive strength and young's modulus, which are determined by the rigid improvement effect of ME nanoparticles [60,61,62].

## 7. Conclusion

Various types of MNP platforms live moment and they're under rapid-fire development. The MNPs can be acclimatized for discovery (MR imaging discrepancy agents) and treatment curatives of colourful conditions, including early- stage and advanced forms of cancer. Face manipulation (silica, gold or biocompatible polymers similar as cut or dextran) can yield stable MNP systems with minimum aggregation or opsonization, furnishing minimum systemic response and a high liability of passage through natural walls (reticuloendothelial, vascular endothelium or blood – brain hedge). Achieving enhanced biocompatibility, precise targeting and increased accumulation of target cells for proper natural response remain the main pretensions. Multifunctional MNPs can offer different remedial strategies for healthcare providers.

Also, a recent exploration direction aims to use glamorous (nano) flyspeck imaging (MPI) in individual imaging and guided treatment remedy, effectively linking image discrepancy and quality to relaxation mechanisms while emphasizing a safety administration profile. With no depth attenuation, MPI grounded on glamorous nano tracers generally SPIONs — could give excellent imaging discrepancy, spatial and temporal resolution and excellent signal- to- noise rate. At its core, the arising field of MPI relies heavily on the successful perpetration of glamorous tracers, and this bid can take advantage of current development in MNPs used for medicine- delivery operations.

## Reference

1. Fadli, A.; Amri, A.; Sari, E.O.; Sukoco, S.; Saprudin, D. Superparamagnetic nanoparticles with mesoporous structure prepared through hydrothermal technique. *Mater. Sci. Forum* **2020**, 1000, 203–209.
2. Ghaemi, A.; Mohave, F.; Farhadi, A.; Takassi, M.A.; Tavakkoli, H. Hydrothermal synthesis of mesoporous cobalt ferrite by ionic liquid-assisted process; catalytic performance, morphology, and magnetic studies. *J. Aust. Ceram. Soc.* **2021**, 57, 1321–1330.
3. Tombuloglu, H.; Khan, F.A.; Almessiere, M.A.; Aldakheel, S.; Baykal, A. Synthesis of niobium substituted cobalt-nickel nanoferrite (Co<sub>0.5</sub>Ni<sub>0.5</sub>Nb<sub>x</sub>Fe<sub>2</sub>□<sub>x</sub>O<sub>4</sub> (x \_ 0.1) by hydrothermal approach show strong anti-colon cancer activities. *J. Biomol. Struct. Dyn.* **2021**, 39, 2257–2265.
4. Panda, J.; Das, S.; Kumar, S.; Tudu, B.; Sarkar, R. Investigation of antibacterial, antioxidant, and anticancer properties of hydrothermally synthesized cobalt ferrite nanoparticles. *Appl. Phys. A Mater. Sci. Process.* **2022**, 128, 562.
5. Albornoz, C.A.; Paulin, M.A.; Cristóbal, A.A.; Vega, D.R.; Leyva, A.G.; Ramos, C.P. Microwave-assisted hydrothermal nanoarchitectonics of polyethyleneimine-coated iron oxide nanoparticles. *Appl. Phys. A Mater. Sci. Process.* **2022**, 128, 68.
6. Fayazzadeh, S.; Khodaei, M.; Arani, M.; Mahdavi, S.R.; Nizamov, T.; Majouga, A. Magnetic Properties and Magnetic Hyperthermia of Cobalt Ferrite Nanoparticles Synthesized by Hydrothermal Method. *J. Supercond. Nov. Magn.* **2020**, 33, 2227–2233.
7. Park, Y.; Yoon, H.J.; Lee, S.E.; Lee, L.P. Multifunctional Cellular Targeting, Molecular Delivery, and Imaging by Integrated Mesoporous-Silica with Optical Nanocrescent Antenna: MONA. *ACS Nano* **2022**, 16, 2013–2023.
8. Wang, F.; Qi, X.; Geng, J.; Liu, X.; Li, D.; Zhang, H.; Zhang, P.; He, X.; Li, B.; Li, Z.; et al. Template-free construction of hollow mesoporous Fe<sub>3</sub>O<sub>4</sub> nanospheres as controlled drug delivery with enhanced drug loading capacity. *J. Mol. Liq.* **2022**, 347, 118000.
9. Gao, Y.; Shi, X.; Shen, M. Intelligent Design of Ultrasmall Iron Oxide Nanoparticle-Based Theranostics. *ACS Appl. Mater. Interfaces* **2021**, 13, 45119–45129.
10. Besenhard, M.O.; Panariello, L.; Kiefer, C.; LaGrow, A.P.; Storozhuk, L.; Perton, F.; Begin, S.; Mertz, D.; Thanh, N.T.K.; Gavriilidis, A. Small iron oxide nanoparticles as MRI T1 contrast agent: Scalable inexpensive water-based synthesis using a flow reactor. *Nanoscale* **2021**, 13, 8795–8805.
11. Gradinaru, L.M.; Mandru, M.B.; Drobot, M.; Aflori, M.; Butnaru, M.; Spiridon, M.; Doroftei, F.; Aradoaei, M.; Ciobanu, R.C.; Vlad, S. Composite materials based on iron oxide nanoparticles and polyurethane for improving the quality of mri. *Polymers* **2021**, 13, 4316.

12. Harvell-Smith, S.; Tung, L.D.; Thanh, N.T.K. Magnetic particle imaging: Tracer development and the biomedical applications of a radiation-free, sensitive, and quantitative imaging modality. *Nanoscale* 2021, 14, 3658–3697.
13. Svenskaya, Y.; Garello, F.; Lengert, E.; Kozlova, A.; Verkhovskii, R.; Bitonto, V.; Ruggiero, M.R.; German, S.; Gorin, D.; Terreno, E. Biodegradable polyelectrolyte/magnetite capsules for MR imaging and magnetic targeting of tumors. *Nanotheranostics* 2021, 5, 362–377.
14. Rosch, E.L.; Zhong, J.; Lak, A.; Liu, Z.; Etkorn, M.; Schilling, M.; Ludwig, F.; Viereck, T.; Lalkens, B. Point-of-need detection of pathogen-specific nucleic acid targets using magnetic particle spectroscopy. *Biosens. Bioelectron.* 2021, 192, 113536.
15. Bruno, F.; Granata, V.; Bellisari, F.C.; Sgalambro, F.; Tommasino, E.; Palumbo, P.; Arrigoni, F.; Cozzi, D.; Grassi, F.; Brunese, M.C., et al. Advanced Magnetic Resonance Imaging (MRI) Techniques: Technical Principles and Applications in Nanomedicine. *Cancers* 2022, 14, 1626.
16. Zhao, Z.; Li, M.; Zeng, J.; Huo, L.; Liu, K.; Wei, R.; Ni, K.; Gao, J. Recent advances in engineering iron oxide nanoparticles for effective magnetic resonance imaging. *Bioact. Mater.* 2022, 12, 214–245.
17. Wu, K.; Liu, J.; Saha, R.; Ma, B.; Su, D.; Peng, C.; Sun, J.; Wang, J.-P. Irregularly Shaped Iron Nitride Nanoparticles as a Potential Candidate for Biomedical Applications: From Synthesis to Characterization. *ACS Omega* 2020, 5, 11756–11767.
18. Yan, Q.; Dong, X.; Xie, R.; Xu, X.; Wang, X.; Zhang, K.; Xia, J.; Ling, J.; Zhou, F.; Sun, J. Preparation of Mn<sup>2+</sup>@PolyDOPA-bpolysarcosine micelle as MRI contrast agent with high longitudinal relaxivity. *J. Macromol. Sci. Part A Pure Appl. Chem.* 2021, 58, 175–181.
19. Ramazanov, M.; Karimova, A.; Shirinova, H. Magnetism for drug delivery, mri and hyperthermia applications: A review. *Biointerface Res. Appl. Chem.* 2021, 11, 8654–8668.
20. Varghese, R.; Vijay, N.; Dalvi, Y.B. *Magnetic Nanoparticles for Image-Guided Drug Delivery. In Magnetic Nanoparticles; Springer: Singapore, 2021; pp. 45–71.*
21. Basina, G.; Diamantopoulos, G.; Devlin, E.; Psycharis, V.; Alhassan, S.M.; Pissas, M.; Hadjipanayis, G.; Tomou, A.; Bouras, A.; Hadjipanayis, C.; et al. LAPONITE@nanodisk-“decorated” Fe<sub>3</sub>O<sub>4</sub> nanoparticles: A biocompatible nano-hybrid with ultrafast magnetic hyperthermia and MRI contrast agent ability. *J. Mater. Chem. B* 2022, 10, 4935.
22. Salunkhe, A.B.; Khot, V.M.; Patil, S.I.; Tofail, S.A.M.; Bauer, J.; Thorat, N.D. MRI Guided Magneto-chemotherapy with High-Magnetic-Moment Iron Oxide Nanoparticles for Cancer Theranostics. *ACS Appl. Bio Mater.* 2020, 3, 2305–2313. Pop, N.L.; Nan, A.; Urda-Cimpean, A.E.; Florea, A.; Toma, V.A.; Moldovan, R.; Decea, N.; Mitrea, D.R.; Orasan, R. Chitosan functionalized magnetic nanoparticles to provide neural regeneration and recovery after experimental model induced peripheral nerve injury. *Biomolecules* 2021, 11, 676.
23. Mohammad Gholiha, H.; Ehsani, M.; Saeidi, A.; Ghadami, A.; Alizadeh, N. Magnetic dual-responsive semi-IPN nanogels based on chitosan/PNVCL and study on BSA release behavior. *Prog. Biomater.* 2021, 10, 173–183.
24. Borges, M.M.C.; Pires, B.C.; Vieira, S.S.; Borges, K.B.; Guimarães, L.G.D.L. Magnetic and pH responsive composite hydrogel-based on poly(2-(diethylamino)ethyl methacrylate)/chitosan for fipronil removal from aqueous medium. *React. Funct. Polym.* 2021, 168, 105050.
25. Cui Y, Xu Q, Chow PK, et al. Transferrin-conjugated magnetic silica PLGA nanoparticles loaded with doxorubicin and paclitaxel for brain glioma treatment. *Biomaterials.* 2013; 34(33):8511–20. [PubMed: 23932498]
26. Lubbe AS, Alexiou C, Bergemann C. Clinical applications of magnetic drug targeting. *J Surg Res.* 2001; 95(2):200–6. Explores magnetic drug targeting for clinical application. [PubMed: 11162046]
27. Li Y, Huang G, Zhang X, et al. Magnetic hydrogels and their potential biomedical applications. *Adv Funct Mater.* 2013; 23(6):660–72.
28. Park H, Yang J, Seo S, et al. Multifunctional nanoparticles for photothermally controlled drug delivery and magnetic resonance imaging enhancement. *Small.* 2008; 4(2):192–6. [PubMed: 18203232]
29. Sangalli D, Cianci E, Lamperti A, et al. Exploiting magnetic properties of Fe doping in zirconia. *Eur Phys J B.* 2013; 86:5.
30. Urbina MC, Zinoveva S, Miller T, et al. Investigation of magnetic nanoparticles polymer composites for multiple-controlled drug delivery. *J Phys Chem C.* 2008; 112(30):11102–8.
31. Veisheh O, Gunn JW, Zhang M. Design and fabrication of magnetic nanoparticles for targeted drug delivery and imaging. *Adv Drug Deliv Rev.* 2010; 62(3):284–304.

32. Pilakka-Kanthikeel S, Atluri VS, Sagar V, et al. Targeted brain derived neurotropic factors (bdnf) delivery across the blood-brain barrier for neuro-protection using magnetic nano carriers: an in-vitro study. *PLoS One*. 2013; 8(4):e62241. This research article highlights delivery of brain derived neurotropic factors delivery across BBBs.
33. Ding H, Sagar V, Agudelo M, et al. Enhanced blood-brain barrier transmigration using a novel transferrin embedded fluorescent magneto-liposome nanoformulation. *Nanotechnology*. 2014; 25(5):055101. Application of magnetic-liposome nanoformulation for enhanced BBB delivery.
34. Ding H, Wu F, Nair MP. Image-guided drug delivery to the brain using nanotechnology. *Drug Discov Today*. 2013; 18(21):1074–80. Discusses image guided drug delivery.
35. Tripathy SN, Mishra B, Shirolkar MM, et al. Structural, microstructural and magneto-electric properties of single-phase BiFeO<sub>3</sub> nanoceramics prepared by auto-combustion method. *Mater Chem Phys*. 2013; 141(1):423–31.
36. Ohno H, Chiba D, Matsukura F, et al. Electric-field control of ferromagnetism. *Nature*. 2000; 408(6815):944–6. Explains properties of ME-NP.
37. Lottermoser T, Lonkai T, Amann U, et al. Magnetic phase control by an electric field. *Nature*. 2004; 430(6999):541–4. Explain properties of ME-NP.
38. Guduru R, Liang P, Runowicz C, et al. Magneto-electric nanoparticles to enable field-controlled high-specificity drug delivery to eradicate ovarian cancer cells. *Sci Rep*. 2013; 3:2953. Paper explores ME-NP based on-controlled drug delivery to cure cancer.
39. Nair M, Guduru R, Liang P, et al. Externally controlled on-demand release of anti-HIV drug using magneto-electric nanoparticles as carriers. *Nat Commun*. 2013; 4:1707. Paper discusses potentials of ME-NP based on-demand controlled drug delivery across BBB.
40. Liu W, Miroshnichenko AE, Neshev DN, et al. Broadband unidirectional scattering by magneto-electric core-shell nanoparticles. *ACS Nano*. 2012; 6(6):5489–97.
41. Guduru R, Khizroev S. Magnetic field controlled release of paclitaxel drug from functionalized magnetoelectric nanoparticles. *Part Syst Char*. 2014; 31:605–11. Describes application of ME-NP for drug delivery.
42. Yue K, Guduru R, Hong J, et al. Magneto-electric nano-particles for non-invasive brain stimulation. *PLoS One*. 2013; 7(9):e44040. This article potential of ME-NP for noninvasive brain stimulation.
43. Guduru R, Liang P, Runowicz C, et al. Magneto-electric nanoparticles to enable field-controlled high-specificity drug delivery to eradicate ovarian cancer cells. *Sci Rep*. 2013; 3:2953. Paper explores ME-NP based on-controlled drug delivery to cure cancer.
44. Ashcroft, FM. Ion channels and disease. Academic press; USA: 1999
45. Xiao, Y.; Du, J. Superparamagnetic nanoparticles for biomedical applications. *J. Mater. Chem. B* 2020, 8, 354–367.
46. Liu, Z.; Liu, J.; Cui, X.; Wang, X.; Zhang, L.; Tang, P. Recent Advances on Magnetic Sensitive Hydrogels in Tissue Engineering. *Front. Chem*. 2020, 8, 124
47. Nuñez-Magos, L.; Lira-Escobedo, J.; Rodríguez-López, R.; Muñoz-Navia, M.; Castillo-Rivera, F.; Viveros-Méndez, P.X.; Araujo, E.; Encinas, A.; Saucedo-Anaya, S.A.; Aranda-Espinoza, S. Effects of DC Magnetic Fields on Magnetoliposomes. *Front. Mol. Biosci*. 2021, 8, 703417.
48. Sriwidodo Umar, A.K.; Wathoni, N.; Zothantluanga, J.H.; Das, S.; Luckanagul, J.A. Liposome-polymer complex for drug delivery system and vaccine stabilization. *Heliyon* 2022, 8, e08934.
49. Novak, E.V.; Pyanzina, E.S.; Gupalo, M.A.; Mauser, N.J.; Kantorovich, S.S. Structural transitions and magnetic response of supramolecular magnetic polymerlike structures with bidisperse monomers. *Phys. Rev. E* 2022, 105, 054601.
50. Iliasov, A.R.; Nizamov, T.R.; Naumenko, V.A.; Garanina, A.S.; Vodopyanov, S.S.; Nikitin, A.A.; Pershina, A.G.; Chernysheva, A.A.; Kan, Y.; Mogilnikov, P.S.; et al. Non-magnetic shell coating of magnetic nanoparticles as key factor of toxicity for cancer cells in a low frequency alternating magnetic field. *Colloids Surf. B* 2021, 206, 111931.
51. Malhotra, N.; Lee, J.-S.; Liman, R.A.D.; Ruallo, J.M.S.; Villaflore, O.B.; Ger, T.-R.; Hsiao, C.-D. Potential toxicity of iron oxide magnetic nanoparticles: A review. *Molecules* 2020, 25, 3159.
52. Kefeni, K.K.; Msagati, T.A.M.; Nkambule, T.T.; Mamba, B.B. Spinel ferrite nanoparticles and nanocomposites for biomedical applications and their toxicity. *Mater. Sci. Eng. C* 2020, 107, 110314.
53. Cervantes, O.; Casillas, N.; Knauth, P.; Lopez, Z.; Virgen-Ortiz, A.; Lozano, O.; Delgado-Enciso, I.; Sámano, A.H.; Rosales, S.; Martinez-Ceseña, L.; et al. An easily prepared ferrofluid with high power absorption density and low cytotoxicity for biomedical applications. *Mater. Chem. Phys*. 2020, 245, 122752. [CrossRef]

54. Toropova, Y.G.; Motorina, D.S.; Gorshkova, M.; Gareev, K.G.; Korolev, D.V.; Muzhikyan, A.A. The effect of intravenous administration to rats of magnetite nanoparticles with various shells on the functional state and morphology of the endothelium and on antioxidant status. *Transl. Med.* 2020, 7, 52–64.
55. Srikanth, K.; Nutalapati, V. Copper ferrite nanoparticles induced cytotoxicity and oxidative stress in Channel catfish ovary cells. *Chemosphere* 2022, 287, 132166.
56. Wang, X.; Zhang, Y.; Tan, W.; Nie, K.; Xu, X. Protective effect of Fe<sub>3</sub>O<sub>4</sub> nanoparticles on cadmium chloride-induced toxicity in the small intestine of mice. *J. Univ. Sci. Technol. China* 2020, 50, 887–893.
57. R.A. Surmenev, M.A. Surmeneva, A.A. Ivanova, Significance of calcium phosphate coatings for the enhancement of new bone osteogenesis – a review, *Acta Biomater.* 10 (2014) 557–579, <https://doi.org/10.1016/j.actbio.2013.10.036>.
58. A. Marino, J. Barsotti, G. de Vito, C. Filippeschi, B. Mazzolai, V. Piazza, M. Labardi, V. Mattoli, G. Ciofani, Two-photon lithography of 3D nanocomposite piezoelectric scaffolds for cell stimulation, *ACS Appl. Mater. Interfaces* 7 (2015) 25574–25579, <https://doi.org/10.1021/acsami.5b08764>.
59. W. Liu, F. Zhang, Y. Yan, C. Zhang, H. Zhao, B. Chin Heng, Y. Huang, Y. Shen, J. Zhang, L. Chen, X. Wen, X. Deng, Remote tuning of built-in magnetoelectric microenvironment to promote bone regeneration by modulating cellular exposure to arginylglycylaspartic acid peptide, *Adv. Funct. Mater.* 31 (2021) 2006226, <https://doi.org/10.1002/adfm.202006226>.
60. C. Shuai, W. Yang, C. He, S. Peng, C. Gao, Y. Yang, F. Qi, P. Feng, A magnetic micro-environment in scaffolds for stimulating bone regeneration, *Mater. Des.* 185 (2020) 108275, <https://doi.org/10.1016/j.matdes.2019.108275>.
61. A. Reizabal, R. Brito-Pereira, M.M. Fernandes, N. Castro, V. Correia, C. Ribeiro, C.M. Costa, L. Perez, J.L. Vilas, S. Lanceros-Mendez, Silk fibroin magnetoactive nanocomposite films and membranes for dynamic bone tissue engineering strategies, *Materialia* 12 (2020) 100709, <https://doi.org/10.1016/j.mtla.2020.100709>.
62. L. Amaro, D.M. Correia, P.M. Martins, G. Botelho, S.A.C. Carabineiro, C. Ribeiro, S. Lanceros-Mendez, Morphology dependence degradation of electroand magnetoactive poly(3-hydroxybutyrate-co-hydroxyvalerate) for tissue engineering applications, *Polymers* 12 (2020) 953, <https://doi.org/10.3390/polym12040953>.